How the embryonic chick brain twists

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During early development, the tubular embryonic chick brain undergoes a combination of progressive ventral bending and rightward torsion, one of the earliest organ-level left–right asymmetry events in development. Existing evidence suggests that bending is caused by differential growth, but the mechanism for the predominantly rightward torsion of the embryonic brain remains poorly understood. Here, we show through a combination of in vitro experiments, a physical model of the embryonic brain tube remains poorly understood. Here, we show through a combination of in vitro experiments, a physical model of the embryonic morphology and mechanics analysis that the vitelline membrane (VM) exerts an external load on the brain that drives torsion. Our theoretical analysis showed that the force is of the order of 10 microns. We also designed an experiment to use fluid surface tension to replace the mechanical role of the VM, and the estimated magnitude of the force owing to surface tension was shown to be consistent with the above theoretical analysis. We further discovered that the asymmetry of the looping heart determines the chirality of the twisted brain via physical mechanisms, demonstrating the mechanical transfer of left–right asymmetry between organs. Our experiments also implied that brain flexure is a necessary condition for torsion. Our work clarifies the mechanical origin of torsion and the development of left–right asymmetry in the early embryonic brain.

1. Introduction

Morphogenesis, the generation of biological form [1], has been studied for centuries. In his classic book, *On growth and form* [2], Thompson suggests that the form of an organism (and its changes) can be ‘explained by the interaction or balance of forces’, calling attention to the need for understanding the mathematical and physical aspects of biological growth and morphogenesis. While modern developmental biologists have mostly focused on the genetic and molecular aspects of development, the search for mathematical and mechanical principles of morphogenesis has never ceased and is currently being revived [3–10].

The transformation of a straight configuration to a chiral shape is ubiquitous in natural and engineered systems [5,11–13]. Although the physical and molecular mechanisms in morphogenesis have been studied for centuries [1–3,5–8,12,14], except for a few studies [15–17], the roles of mechanical forces in early brain morphogenesis are still poorly understood. In particular, the fundamental mechanism underlying the torsion of the embryonic brain [18], one of the earliest morphogenetic events of left–right (L–R) asymmetry in the embryo, remains elusive. Significant birth defects can result when the process of L–R specification is perturbed, including *situs inversus* (inversion of the positions of visceral organs), isomerism (mirror image symmetry of bilaterally asymmetric tissues) and heterotaxia (random and independent occurrence of laterality defects in different tissues) [19].

At Hamburger & Hamilton [20] (HH) stage 10 (after approx. 33 h of incubation), the neural tube of the chick embryo is nearly straight. The anterior
Previous studies have suggested that bending of the brain tube could be attributed in part to differential growth [22], but the biomechanical mechanism of brain torsion remains poorly understood. Interestingly, the heart almost always loops in the same direction (to the right side) that the brain twists, leading some researchers to speculate that the looping heart affects the direction of brain torsion [23,24]. Nevertheless, little direct evidence exists, and the mechanical origin of brain torsion remains elusive.

Here, we use experiments in developing chick embryos and a physical model to show that (i) the vitelline membrane (VM) exerts a mechanical load that causes the brain tube to twist as it bends, (ii) the direction of the looping heart determines the direction of torsion, and (iii) brain flexure is a necessary condition for torsion.

2. Results

2.1. The vitelline membrane applies the compressive load necessary for torsion

In a normal HH11 chick embryo (after approx. 40–45 h of incubation), the embryonic brain tube has not yet begun to twist (figure 1a). After around 20 h of cultivation (to approx. HH stage 16), the brain tube is bent and twisted rightward, whereas the spinal cord is still in its original orientation (figure 1b). A thin membrane called the VM, which is under tension, constrains the embryo on its original dorsal side, and the splanchnopleure (SPL) membrane constrains the heart on the ventral side (figure 1c). Studies have shown that the SPL membrane is a primary cause of torsion of the looping heart [25].

To determine whether the VM, an often-overlooked developmental structure, plays a mechanical role in brain morphogenesis, we removed this membrane before the onset of torsion. More specifically, the VM was cut from the anterior end of the embryo to the spinal cord at the point of the thoracic flexure (figure 2a). Notably, embryos (starting from stage HH11, as shown in figure 2a; n = 12, where n is the number of embryos tested) cultivated for 27 h to HH stage 17 without the dorsal constraint of the VM exhibited considerably less torsion than control embryos. For example, the torsional angle near the eyes \( \approx \) 34 degrees in an embryo shown in figure 2b (see electronic supplementary material, texts and figure S3 for the method of measuring the torsional angle) when compared with the torsional angle \( \approx \) 88 degrees in a control embryo (figure 2f). Furthermore, when we lowered the fluid level in the Petri dish to apply surface tension to the embryo (i.e. when the embryonic brain is exposed to the air–fluid interface it becomes subjected to the fluid surface tension) [26], we found that the brain instantaneously twisted rightward (figure 2c and electronic supplementary material, movie S2), with degrees of torsion similar to the control embryos (e.g. the one in figure 2f). In addition, embryos with the VM removed at HH11 and subjected to surface tension from the culture media showed a similar degree of torsion after another 20 h of cultivation (figure 2c) in that case the surface tension again replaces the mechanical role of the VM in inducing normal torsion. Taken together, these results suggest that the VM applies compressive loads necessary for normal brain
2.2. The direction of the looping heart determines the direction of the twisting brain

In general, the embryonic chick brain twists in the same direction that the heart loops [23], leading researchers to speculate that the looping direction of the heart affects the direction of brain torsion [23,24,27]. To test this hypothesis, we pushed the rightward-looped heart (figure 3a) to the left in stage 11–12 embryos (figure 3b). The SPL held the heart in this position. After 17–25 h of cultivation, the brains in all of these embryos (n = 16) twisted abnormally to the left (figure 3c).

These results support the hypothesis that the twisting direction of the brain tube is determined by the direction of heart looping. When these experiments were repeated with surface tension replacing the mechanical role of SPL, the embryos still all turned leftward (n = 7), implying a fundamental mechanical basis for the transfer of chirality between the heart and brain of the embryonic chick.

We tried to repeat these experiments in embryos at later stages (e.g. HH stage 13 or beyond) in which brain torsion was already significant. At the most advanced stage of development, however, the displaced heart did not remain on the left side, and all the embryonic brains still turned rightward (figure 3d–f). A detailed examination showed that for a stage 13 embryo (or older), the mechanically displaced heart gradually returned to the right side (within a minute or two) as the heart beat (electronic supplementary material, movie S3), and normal brain torsion resumed. Taken together, these results suggest that the direction of heart looping determines the direction of brain torsion, with rightward looping inducing rightward brain torsion, and leftward looping inducing leftward brain torsion. Because the heart predominantly loops to the right side (more than 99% in ovo [23]), it follows that the embryonic brain usually twists rightward.

To further understand how the heart affects brain torsion, we constructed a physical model (see Methods). The model is based on simplified geometry for a chick embryo at HH stage 14–17 without the VM (figure 2b). The embryonic brain is modelled as a curved rod with an elliptical cross section and prescribed intrinsic curvatures (for simplicity, we have just used a circular rod with the same magnitude of the radius, figure 4a,b). The heart is modelled as another curved rod looped towards the right side and constrained by contact with a block representing the SPL (figure 4c,d). A mechanical load is applied at the top of the physical model by a coverslip representing the VM (figure 4d), which is moved downward to compress the brain. Figure 4d shows a slight rightward twisting of the chick embryo model (with the heart looped rightward) subjected to a moderate mechanical load along the gravity direction from the top. Both the physical model and the embryo exhibit similar rightward twisting when the heart loops to the right side, in support of our hypothesis. Figure 4e shows the deformed shape of the physical model when subjected to a larger force from the coverslip than in figure 4d, exhibiting a more significant rightward torsion than in figure 4d, comparable to that in a HH 14 chick embryo.

Ideally, the model without the heart is L–R symmetric, and the brain bends without twisting. With the heart looped to the right side, however, the embryo becomes L–R asymmetric, and the brain tube twists rightward (figure 4d,e). On the other hand, if the heart loops to the left (electronic supplementary material, movie S4) or is pushed to the left side (figure 3e–c), then the brain twists leftward. The reason for this behaviour is that the ventral motion of the heart is constrained by the SPL, causing the heart to push the brain tube leftward at the point where these organs are connected. This force exerts a torque relative to the fixed spinal cord, causing the brain to twist rightward relative to its body axis. Simply put, the presence of the heart breaks the symmetry and causes the brain to twist asymmetrically relative to the fixed spinal cord region when subjected to external forces from either the VM or surface tension. These results are consistent with our previous experiments, lending support to the hypotheses that the VM applies a mechanical load necessary for brain torsion, whereas the looping direction of the heart determines the chirality of the twist.

2.3. Brain flexure is another requisite condition for torsion

Inspired by the work of Manners et al. [28], we implanted an eyelash into the lumen of the brain tube to suppress flexure in order to study the relationship between brain bending
and torsion. The eyelash was implanted in the brain tube at HH stage 11 (figure 3g, n = 7) to reach at least the second somite, and the embryo was cultivated for approximately 18 h. Much less torsion of the brain tube was observed (figure 3i; torsional angle $\approx 35$ degrees) when compared with an unperturbed embryo (figure 3i; torsional angle $\approx 88$ degrees) or a control embryo (with an eyelash implanted and removed immediately at HH11) cultivated to a similar stage (figure 3j; torsional angle $\approx 88$ degrees). These results suggest that the development of curvatures in the brain tube is also a necessary condition for normal brain torsion to occur.

It is noteworthy that, in addition to the cranial and cervical flexures, a third flexure develops in the neural tube. This flexure occurs posterior to cervical flexure and near the anterior part of the spinal cord, and bends the embryo in a direction opposite to the cranial and cervical flexures (figures 1b and 2h,c). This otherwise overlooked flexure, namely the ‘thoracic flexure’, is still visible in embryos with the VM removed (figure 2b,c), as well as in rat and mouse embryos [27,29]. We found that the thoracic and cervical flexures play an important role in the development of brain torsion. When these flexures were suppressed by implantation of an eyelash much stiffer than the embryonic tissues, brain torsion was also significantly suppressed (figure 3h). However, when only the cranial flexure was suppressed by an implanted eyelash not reaching the first somite (figure 3j; n = 7), the embryo still turned rightward (figure 3k), exhibiting a comparable degree of torsion (torsional angle $\approx 83$ degrees) to a normal embryo (figure 3i; torsional angle $\approx 88$ degrees) or a control embryo (figure 3l). Therefore, the development of thoracic and cervical flexures constitute a requisite condition for normal brain torsion, but not the other way around, i.e. even if brain torsion was dramatically reduced (figure 2h), the magnitudes of the flexures were not significantly affected.
2.4. Estimation of the magnitude of the force

The VM, acting as a mechanical boundary for the growing embryonic brain tube, was shown to be a necessary structure for the twisting of the brain. In particular, the passive downward force of the VM was shown to be fundamental in this role: the brain no longer twisted to a normal degree when the VM of the embryo was removed, but could be made to twist to control levels through the application of surface tension force from lowering culture fluid levels. Because the surface tension of water at the ambient temperature is $72.01 \pm 0.1 $ mN m$^{-1}$ [30], and the contact length is on the order of millimetres, the force

$$ F \approx 72 \times 10^{-3} \cdot N \cdot m^{-1} \times 10^{-3} \cdot m \approx 10^{-5} \cdot N = 10 \mu N. $$

Thus, we determine that the VM exerts a force of approximately $10 \mu N$ on the HH 14–17 embryo. Alternatively, $F$ can be estimated as by considering the balance of the torque

$$ F \times 2R \approx GJ \tau = \frac{GJ}{2R}, $$

where $R$ is the radius of curvature for all flexures (assuming all flexures have the same curvature), $G$ is the shear modulus and $J$ is the cross-sectional polar moment of inertia. The torsion is $\tau = \pi R^2 / (2R)$ when the embryo is twisted by $\pi / 2$.

Therefore,

$$ F \approx \frac{GJ}{4R^2} = \frac{G(\pi l^4 / 32)}{4R^2}. $$

Using the following estimated values: $G \approx 200$ Pa, $d \approx 1.8$ mm and $R \approx 1.5$ mm, it follows that $F \approx 10 \mu N$, consistent with the previous estimated value using the surface tension.

3. Discussion

In this study, we demonstrated through experiments and a physical model that the combination of the rightward looping heart and the physical constraint of the VM are necessary and sufficient conditions for the rightward torsion of the ventrally flexed brain tube of the chick embryo.

The cervical and thoracic flexures were also shown to be necessary conditions for the development of torsion. When these flexures were allowed to develop normally, torsion also proceeded normally; however, when these flexures were suppressed through the axial implantation of an eyelash, torsion was drastically attenuated. We can verify that the insertion of the eyelashes forcibly suppresses the curvature of the embryonic body by comparing the relative bending sti\(ff\)nesses of the two objects. The linear elastic modulus of the embryonic midline structures at HH 10 has been measured at $2.4 \pm 0.1$ kPa [31], whereas the linear elastic modulus of human hair is approximately 9.5 GPa [32]. The bending rigidity of a circular rod is

$$ EI \approx Ed^4, $$

where $E$ is the linear elasticity, $I$ is the moment of inertia and $d$ is the beam diameter. Therefore,

$$ \frac{(EI)_{\text{eyelash}}}{(EI)_{\text{embryo}}} \approx 10^6 \times \left( \frac{d_{\text{eyelash}}}{d_{\text{embryo}}} \right)^4 \approx 10^2 \gg 1, $$

where $d_{\text{eyelash}} / d_{\text{embryo}} \approx 0.1$. In other words, the bending rigidity of the inserted eyelash is two orders of magnitude higher than the embryo and thus effectively suppresses the flexure of the embryonic brain.

From a broader perspective, spontaneous chiral structures are ubiquitous in natural and engineering structures, from the DNA double helix to looping guts [5], from chiral seed pods [11] and plant tendrils [12,33,34] to strained multilayer composites [11,13,35,36] and curly hair [37], where a variety of mechanical or biophysical mechanisms are operating. Morphogenesis is a complex biophysical process, whereby mechanical cues interact with molecular mechanisms in an exquisitely orchestrated fashion to regulate the shaping of functional biological form [1,3,7]. Within the transforming growth factor TGF-β family, lefty and nodal are known to play important roles in the determination and maintenance of L–R asymmetry [38,39]. While gene expression and molecular signalling are certainly central to embryonic development, the role of mechanical forces in morphogenesis has been increasingly acknowledged [3,5–8]. For example, Savin et al. [5] discovered that forces generated by different growth rates between the gut tube and the adjacent dorsal mesenteric sheet drive the morphogenesis of gut looping. More recently, Shy et al. revealed the role of mechanical stresses in the formation of villi in the gut [8]. Forces extrinsic to the primitive heart tube also are important players during cardiac looping [14,26,40,41]. Results from these studies suggest that the SPL plays a mechanical role in facilitating cardiac torsion that may be similar to the role of the VM in inducing brain torsion. A more recent study implies that both differential contractility and stress-dependent growth play key roles in early brain morphogenesis [42].

Axial rotation of the neural tube is among the earliest tissue-level events that breaks LR symmetry in the developing embryos [18], following the rightward looping of the heart. In amniote embryos, such as chicken and mice [19], brain torsion typically begins a few hours after cardiac looping begins. Severe defects can result when the process of LR specification is perturbed, including situs inversus (inversion of the positions of visceral organs), isomerism (mirror image symmetry of bilaterally asymmetric tissues) and heterotaxia (random and independent occurrence of laterality defects in different tissues) [19].

The detailed mechanisms of axial rotation may vary because of different amounts of yolk present in different species. In yolk-less mammalian embryos, such as those of a rat or mouse, the embryonic axis first develops a ‘U’ shape with the outer curvature of the embryo being ventral and the inner curvature being dorsal [43]. Then, at a species-dependent stage (from 10.5 to 11.5 days in the rat and from 8.5 to 9.5 days in the mouse), the embryo rotates about its axis so that the dorsoventral orientation of the curvature inverts. During this process, the head turns rightward as in the avian embryo. In this case, however, the rotational angle is 180 degrees, in contrast to the 90-degree turn in yolk-rich avian embryos, where the constraint of the yolk prevents further rotation. The fundamental mechanism behind axial rotation in mammalian embryos is still poorly understood. It has been suggested that differential growth owing to asymmetric cell proliferation causes this rotation. Some investigators have speculated that the extraembryonic membranes and the beating heart play important roles in regulating axial rotation [27,29,43]. However, the contributions of these factors to axial rotation and their interplay require further study before definitive conclusions can be drawn.

In normal chick embryos, the brain tube twisted into a left-handed helix just after the heart loops into a left-handed
helix [28]. In a sense, this process can be considered as a transfer of chirality or LR asymmetry, from the heart to the brain tube through mechanics. Following the first phase of cardiac looping (c-looping), brain torsion in turn ensures the normal helical looping of the heart during the subsequent s-looping [41]. This type of transfer of chirality between two co-developing organs at the same length scale has not previously been examined in detail, although the transfer of chirality from microscopic-to-macroscopic scale in plant tendrils has recently been studied [34]. It is worth noting that in murine embryos, the LR asymmetry of the developing heart might also affect axial rotation of the embryo [43]. It has been suggested that the neural tube itself may not be the motor that drives torsion; instead, the coordinated activity of somites may play a role [29]. In biological systems, chirality can transfer from the microscopic level (such as in the cytoskeleton) [44] to the cell, tissue and organism level [45], but whether this principle applies to chirality generation in embryonic axial rotation remains unknown.

It also remains to be examined how mechanical and molecular mechanisms interact and coordinate to regulate morphogenesis. For example, Manca et al. [46] recently discovered that nerve growth factor (NGF) regulates axial rotation in chick embryos, as injection of an anti-NGF antibody induces a dose-dependent inversion of rotation direction. Specifically, a high dose causes a remarkable change in the direction of rotation to the left side (reversed torsion). Nevertheless, it is unclear whether NGF regulation works directly or indirectly on axial rotation in chick embryos, because misdirection of heart looping can also reverse the rotation direction of the brain.

Moreover, researchers have proposed that the axial rotation in mammalian embryos is correlated with asymmetry in the developing heart [43] and asymmetric mitotic activity in the developing neural tube [47]. Abnormal looping direction in the heart often occurs concurrently with reversed turning of the embryo [46], suggesting the correlation between heart torsion and axial rotation directions may also exist in mammalian embryos.

However, the role of mechanical stresses in axial rotation of mammalian embryos remains poorly understood. Presumably, the 180-degree turn in murine embryos should be more difficult than the 90-degree turn in avian embryos. Nevertheless, axial rotation in mouse embryos finishes at the 13-somite stage, whereas in chick embryos, this process is not completed until HH stage 20 with around 40–43 somites. We speculate that mechanical forces also play an important role in the axial rotation of murine embryos. Possibly involved are the mechanical factors related to constraints from the extraembryonic membranes and the asymmetrically looped heart, because the heart also normally loops to the right and the head turns rightward in normal murine embryos.

Notably, both thoracic flexure and cranial flexure are even more significant in rodents before the axial rotation starts (evidenced by the ‘U’ shape), which suggests that some mechanical mechanism similar to that in avian embryos could be operating. Further important insights can be gained by studying embryos with defects in axial rotation, for example, chick embryos with misexpression of the Cerberus (cCer) gene (related genes include Xenopus Cebus and mouse mCer-I/mCer-I) [49], mutant mouse embryos such as fur [50] and no turning (nt) [51], or embryos lacking in the gene rotatin [19].

Collectively, our study shows that normal brain torsion in the chick embryo requires at least three mechanical conditions: pressure exerted by the VM; rightward looping of the heart that dictates the brain torsion direction and appropriate neural tube flexures, especially cervical and thoracic flexures. Our experiments and simulations confirm that the torsion direction is determined by the heart-looping direction, demonstrating a transfer and amplification of L–R asymmetry through mechanics. In return, the increasing brain torsion may provide the mechanical forces necessary for the normal morphogenesis of cardiac s-looping [41], such that these two torsional morphogenetic events reinforce each other to ensure normal development. Furthermore, we found that the traditionally overlooked thoracic flexure, together with cervical flexure, plays a key role in inducing brain torsion. By considering the balance of torque, the force from the VM is estimated to be in the order of 10 micro-newtons, consistent with the estimate made by calculating the alternative force from the fluid surface tension. This work clarifies the mechanical origins of brain torsion and the associated propagation of L–R asymmetry in avian embryos, thus providing a new biomechanical example recapitulating Thompson’s view of biological form as a ‘diagram of forces’ [2]. Our study also raises questions about how mechanical and biomolecular mechanisms co-regulate morphogenesis and how they have evolved or been preserved across species, inviting further investigations.

4. Methods

4.1. Embryo culture

Fertilized White Leghorn chicken eggs were incubated in a humidified atmosphere at 38°C for 40–48 h to yield embryos at Hamburger and Hamilton (HH) stages 11–13 [25]. Whole embryos were harvested from the eggs using a filter paper carrier method [40]. Each embryo was then placed either dorsal or ventral side up in a 35 mm culture dish, completely submerged under a thin layer of liquid culture media, and then incubated at 38°C in 95% O2 and 5% CO2. To preserve humidity, several drops of deionized water were put into the bag containing the culture dish before placing the sealed bag into the incubator. In control embryos, all membranes were kept intact, thus preserving the normal stresses present in the tissue. For mechanical perturbations, microsurgical operations were performed, using fine glass needles. The embryos were subjected to surface tension forces when exposed to air [40]; therefore, by controlling the air–medium interface, the surface tension can be tuned (electronic supplementary material, movie S2). Moreover, the measurement of the torsional angle from the optical coherent tomograph images is illustrated in extended data (figure 1). Despite the consistent results from experiments with embryos that we have drawn our conclusions on, we recognize the limitations set by the paper culture method used, because abnormalities can occur especially when the development of blood vessels is hindered by the surrounding filter paper. Abnormal growth, such as underdevelopment or observed decay in tissue health, is expected and can occur for various reasons. As such, abnormal embryos were often excluded from the study because they cannot ensure a control in variables beyond the variable being perturbed, such as the removal of the VM. As with most experiments with embryos using the paper culture method, embryonic health is determined through observation. Similarly, experiments that investigated the chirality of the brain torsion owing to the direction of the looping heart could be expanded...
4.2. Imaging

Bright-field images were acquired, using a dissecting microscope (Leica M28). A Thorlabs (Newton, NJ) optical coherence tomography system with attached Nikon FN1 microscope was used to acquire cross-sectional image stacks of live embryos. Images were obtained in a 3 mm × 10 mm × 3 mm scanning domain, then processed in ImageJ. The image of the three-dimensional model was taken with a digital single-lens reflex camera (EOS Rebel T3i).

4.3. Physical model

To further illustrate the torsion mechanism, we created a physical model of the embryo. A three-dimensional model of the embryonic morphology was developed in commercial software, COMSOL MULTIPHYSICS. A negative mould of the model was then developed in Rhino 5 by applying Boolean subtraction of the three-dimensional model of the chick embryo from a larger block and splitting the resulting block into three attachable blocks. Following this, we used a three-dimensional printer (MakerGear M2, made by MakerBot, Inc.) loaded with 1.75 mm acrylonitrile butadiene styrene filament to three-dimensional print the negative mould. To cast the mould, we used a fast curing, soft silicone elastomer (EcoFlex 00-50, purchased from Smooth-On, Inc.). We measured and combined equal parts of the two elastomer agents at room temperature, approximately 7.0 g of each agent, and poured the mixture into the mould slowly and evenly from a single point to minimize air bubble formation. We then clamped the mould shut and allowed the EcoFlex to cure for 12 h at room temperature.

References


